

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization
International Bureau



(43) International Publication Date
18 October 2001 (18.10.2001)

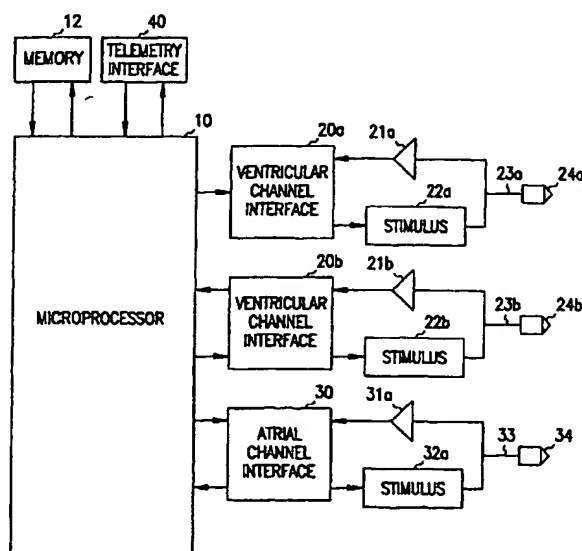
PCT

(10) International Publication Number
WO 01/76689 A2

- (51) International Patent Classification⁷: A61N 1/00 (74) Agent: VIKSNINS, Ann, S.; Schwegman, Lundberg, Woessner & Kluth, P.O. Box 2938, Minneapolis, MN 55402 (US).
- (21) International Application Number: PCT/US01/40415
- (22) International Filing Date: 30 March 2001 (30.03.2001) (81) Designated States (*national*): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, UZ, VN, YU, ZA, ZW.
- (25) Filing Language: English
- (26) Publication Language: English
- (30) Priority Data:
09/544,363 6 April 2000 (06.04.2000) US (84) Designated States (*regional*): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).
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- Published:
— without international search report and to be republished upon receipt of that report

[Continued on next page]

(54) Title: SYSTEM FOR SPATIALLY AND TEMPORALLY DISTRIBUTING CARDIAC STIMULATION



(57) Abstract: A cardiac electro-stimulatory device and method for operating same in which stimulation pulses are distributed among a plurality of electrodes fixed at different sites of the myocardium in order to reduce myocardial hypertrophy brought about by repeated pacing at a single site and/or increase myocardial contractility. In order to spatially and temporally distributes the stimulation, the pulses are delivered through a switchable pulse output configuration during a single cardiac cycle, with each configuration comprising one or more electrodes fixed to different sites in the myocardium.

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SYSTEM FOR SPATIALLY AND TEMPORALLY DISTRIBUTING CARDIAC STIMULATION

Field of the Invention

This invention pertains to apparatus and methods for electrostimulation of the heart including cardiac pacing with an artificial pacemaker. In particular, the invention relates to the manner in which electrical stimulation is delivered to
5 the heart.

Background

Conventional cardiac pacing with implanted pacemakers involves excitatory electrical stimulation of the heart by an electrode in electrical contact with the myocardium. (As the term is used herein, "excitatory stimulation"
10 refers to stimulation intended to cause a cardiac contraction.) The pacemaker is usually implanted subcutaneously on the patient's chest, and is connected to an electrode for each paced heart chamber by leads threaded through the vessels of the upper venous system into the heart. In response to sensed electrical cardiac events and elapsed time intervals, the pacemaker delivers to the myocardium a
15 depolarizing voltage pulse of sufficient magnitude and duration to cause an action potential. A wave of depolarizing excitation then propagates through the myocardium, resulting in a heartbeat.

The normal rhythmic impulse of the heart is first generated in pacemaker tissue known as the sino-atrial (SA) node, spreads throughout the atria causing
20 atrial contraction, and is then conducted to the atrioventricular (AV) node where the impulse is delayed before passing into the ventricles. The ventricles of a normal heart are then electrically stimulated by excitation emanating from the AV node that spreads to the heart via specialized conduction pathways known as Purkinje fibers. These fibers lie beneath the endocardium and spread throughout
25 each ventricular chamber where they penetrate into the myocardium and become continuous with the muscle fibers. The conduction velocity of the Purkinje fibers is very rapid so that the time between the impulse leaving the AV node and spreading to the entire endocardial surface of the ventricles is only approximately .03 seconds. Once the impulse has reached the ends of the

Purkinje fibers, it is then transmitted through the ventricular muscle mass by the muscle fibers themselves with a conduction velocity only about one-sixth that of the Purkinje fibers. Because of the rapid excitation of the entire endocardial surface by the Purkinje system, however, the spread of excitation from the endocardial surface to the epicardial surface of the ventricles takes only about another .03 seconds. This means that in the normal heart, excitation of the first ventricular muscle fiber occurs only about .06 seconds before the last ventricular muscle fiber is excited. The result is a synchronous contraction in which all portions of the ventricular muscle in both ventricles begin contracting at nearly the same time. Not only does this increase the pumping efficiency of the ventricles, but it also evenly distributes ventricular wall stress during the pumping cycle.

Unfortunately, artificial ventricular pacing with an electrode fixed into an area of the myocardium cannot take advantage of the heart's normal Purkinje conduction system because that system can only be entered by impulses emanating from the AV node. Thus the spread of excitation must proceed only via the much slower conducting ventricular muscle fibers, resulting in the part of the ventricular myocardium stimulated by the pacing electrode contracting well before parts of the ventricle located more distally to the electrode. Although the pumping efficiency of the heart is somewhat reduced from the optimum, most patients can still maintain more than adequate cardiac output with artificial pacing.

Another deleterious effect of the conduction delays brought about by artificial pacing, however, is the uneven distribution of wall stress during the cardiac pumping cycle. The degree of tension on a heart muscle fiber before it begins to contract is termed the preload. Because pressure within the ventricles rises rapidly from a diastolic to a systolic value as blood is pumped out into the aorta and pulmonary arteries, the part of the ventricle that first contracts due to a pacing pulse does so against a lower pressure preload than does a part of the ventricle contracting later which unevenly stresses the myocardium. The heart's physiological response to this uneven preload and stress is compensatory hypertrophy in the areas of the myocardium that must contract against a greater pressure load. Not only can this hypertrophy cause blood flow problems that

may further hinder pumping efficiency, but it has been found that myocytes (i.e., cardiac muscle cells) which are made to contract against a greater than normal mechanical load can be induced to undergo apoptosis (i.e., genetically programmed cell death). This may be especially true in pacemaker patients, a large proportion of whom do not have healthy myocardium to begin with, most commonly as a result of ischemic heart disease.

Summary of the Invention

The present invention is a method and apparatus for cardiac stimulation that spatially and temporally distributes electrical stimulation to more than one site of either the atria or ventricles. One embodiment involves distributing excitatory electrical stimulation for pacing the heart with an artificial pacemaker. A primary objective in distributing the pacing to multiple sites is to reduce disparities in the distribution of preload and stress during systole to thereby reduce compensatory hypertrophy of the myocardium and/or apoptosis of myocytes. In one embodiment, a plurality of pacing electrodes are fixed at separate sites, and a selected electrode or group of electrodes among the plurality are energized during any one cardiac cycle. The selected electrode or electrodes used to stimulate the heart chamber may then be switched to a different electrode or group of electrodes on a beat-to-beat basis, at fixed time intervals, or in accordance with a sensed parameter. A particular mode of practicing the invention can also be implemented with a conventional pacemaker having a single bipolar pacing electrode for pacing a particular heart chamber and control circuitry for changing the polarity of the electrode in accordance with a switching algorithm.

In another embodiment, non-excitatory electrical stimulation is distributed over the myocardium similar to the distributed pacing described above. In this case, however, rather than pacing the heart, the stimulation is employed to enhance myocardial contractility by delivering stimulatory electrical pulses synchronized with intrinsic cardiac activity and during the myocardial refractory period. Such stimulation may be delivered either by a specialized electro-stimulatory device or a pacemaker configured to deliver non-excitatory stimulation to the heart.

Brief Description of the Drawings

Fig. 1 is a block diagram of an exemplary electro-stimulatory cardiac device for practicing the present invention.

Fig. 2 shows a bipolar electrode.

5 Description of the Invention

In accordance with the invention, an electro-stimulatory device spatially and temporally distributes stimulatory pulses to multiple sites of either the atria or ventricles by switching between different electrode configurations. Such electro-stimulatory devices include both devices for pacing the heart with
10 excitatory stimulation (i.e., artificial pacemakers) as well as devices for delivering non-excitatory stimulation pulses to the heart. Furthermore, the term should be taken to include any cardiac rhythm management device, such as an implantable cardioverter/defibrillator, with a pacing or non-excitatory stimulation function incorporated therein.

15 Pacemakers have been constructed for delivering pacing pulses to multiple ventricular or atrial sites, including so-called biventricular pacemakers where pacing pulses are delivered to both ventricles by separate electrodes during a cardiac cycle. (See, e.g., U.S. Patent Nos. 5,792,203 and 4,928,688, referred to herein as the '203 and '688 patents, which are hereby incorporated by
20 reference.) One type of multi-site pacing involves fixing two or more pacing electrodes to separate sites of the same heart chamber, either an atrium or a ventricle. For example, one electrode may be fixed to the apical region of either the right or left ventricle with the other electrode fixed to a basal region of the same ventricle. In the case of the left ventricle, this may be most easily
25 accomplished by using a coronary sinus lead (See U.S. Patent No. 5,935,160, hereby incorporated by reference) with distal and proximal electrodes. The ventricle can be paced in accordance with a programmed pacing mode with the electrodes being energized simultaneously during each pacing output in order to achieve near simultaneous activation of the ventricle. Alternatively, the pacing
30 stimuli can be delivered to the ventricular electrodes sequentially with a specified time delay in order to take into account differing conduction times within the ventricle.

Biventricular pacemakers, such as described in the '688 patent, provide pacing to both ventricles in the presence of an interventricular conduction defect. Biventricular pacing may also be useful in certain instances, however, when interventricular conduction pathways are intact. For example, a

5 biventricular pacemaker of the kind described in the '688 patent can be configured with one electrode pacing the posterior or lateral wall of the left ventricle and the other electrode pacing the apex of the right ventricle. When only the left ventricular site is paced, the spread of activation is from the paced site as well as from the part of the normal left ventricular conduction system that

10 is still intact (which would be in the vicinity of the basal region of the interventricular septum). Thus, although only one site is paced, the spread of activation is from two sites. If, on the other hand, both sites are paced, either simultaneously or with a specified interventricular delay between the right and left ventricles, a similar spread of activation occurs from the left ventricular site,

15 but a changed activation occurs from the right ventricular site that breaks through into the left ventricle somewhere in the apical region of the interventricular septum. There is thus left ventricular activation spreading from two (or more) sites which is different from the activation that occurs with left ventricular pacing alone. By adjusting the interventricular delay, the relative

20 spread of activation between the two pacing sites can be modified which thereby affects the wall stress developed near these sites and throughout the ventricle during contraction.

Multi-site pacemakers such as described in the '688 and '203 patents are capable of delivering pacing stimuli to multiple sites of the atria or ventricles in

25 which the multiple sites are all stimulated during any one cardiac cycle. Each of the pulses delivered to the multiple pacing sites during the cardiac cycle, however, must be of sufficient energy (i.e., sufficient pulse amplitude and duration) to cause heart muscle contraction were it to be delivered alone, since pacing stimuli applied over a wide area cannot sum together. Both because of

30 increased battery requirements and the physiological effects on the heart, therefore, it may not be desirable to deliver simultaneous pacing at multiple sites. Furthermore, certain patients may benefit from activating parts of the ventricle at different times in order to distribute the pumping load to different

areas of the ventricle. For example, a relatively weak area of the myocardium could be activated before stronger areas to result in a distribution of wall stress that increases pumping efficiency. In any of the situations discussed above, therefore, it may be desirable to spatially and temporally distribute the pacing.

- 5 In accordance with the invention, a multi-site pacemaker accomplishes this objective by switching the output of pacing pulses between selected electrodes or groups of electrodes during different cardiac cycles.

Another useful application of spatial/temporal switching is to distribute the effects of localized multi-site stimulation pulses that can improve myocardial
10 contractility. (See Braunwald et al., *Sustained paired electrical stimuli; Slowing of the ventricular rate and augmentation of contractile force*, American Journal of Cardiology 14:385, 1964; Sabbah, et al., *Delivery of Non-excitatory Contractility-Modulation Electric Signals Improve Left Ventricular Performance in Dogs with Heart Failure*, Circulation Supplement 1, Vol. 100, pg. I-122,
15 Abstract 631, November 2, 1999). In this type of pacing, multiple pulses are output to a pacing electrode during one or more phases of the action potential in order to improve local contractile function. For example, a non-excitatory stimulating pulse could be applied after a pacing pulse and during the absolute refractory period to increase intracellular calcium concentration which thereby
20 enhances contractility. Because this type of stimulation also increases local oxygen consumption, switching the stimulation site by spatially and temporally distributing the stimulation in accordance with the present invention serves to help prevent deleterious effects at the pacing site. Such effects may be due to biological adaptation resulting from expression of intracellular proteins involved
25 in ion transport and contractile function.

Cardiac pacemakers stimulate the heart by delivering a voltage pulse to an electrode situated on or in the myocardium, with the stimulating electrode usually acting as a cathode. The electrode may be "fixed" to a heart chamber in one of three basic ways: it may be left to float inside one of the heart chambers
30 near the heart wall, actively fixed in the myocardium by implantation, or passively fixed against the endocardium via a tissue encapsulation reaction. In order to pace the heart, the electrode must deliver a voltage pulse of sufficient magnitude and duration to cause a propagated action potential resulting in a

contraction of the myocardium (i.e., an excitatory stimulation). In accordance with the invention, pacing is delivered to a heart chamber through a switchable configuration of pacing electrodes, wherein a pulse output configuration is defined as a specific subset of a plurality of electrodes fixed to the paced
5 chamber and to which pacing pulses are applied. A plurality of different pulse output configurations may be defined as subsets of electrodes that can be selected for pacing. By switching the pulse output configuration to a different configuration, pacing to the heart chamber is thereby temporally distributed among the total number of fixed electrodes. For example, two electrodes may
10 be fixed to a heart chamber with each electrode constituting a pulse output configuration, and switching the pulse output configuration alternately between the electrodes.

In various embodiments of the invention, a particular electro-stimulatory configuration may comprise one or more electrodes, and a particular electrode
15 may belong to one or more configurations. A plurality of different pulse output configurations may then be defined as subsets of the total number of stimulatory (for pacing or non-excitatory stimulation) electrodes fixed to the paced heart chamber. For example, the pacemaker may have N ventricular stimulatory electrodes with a particular subset n of those electrodes selected for pacing in a
20 particular pulse output configuration, so that stimuli are applied to n different sites in the ventricle during a cardiac cycle. In accordance with a particular switching algorithm, the pulse output configuration may then be switched to a different subset m of the N channels to spatially and temporally distribute the stimulation. The subset m making up the configuration that is switched to may
25 be any combination of the N electrodes. That is, the number of electrodes in the subset m may be the same or different as the number of electrodes in the subset n , and the two subsets may have electrodes in common. A pulse output configuration may also be further defined as a particular temporal sequence of pacing or non-excitatory stimulation pulses applied to the electrodes making up
30 the configuration. For example, a pulse output configuration may consist of two electrodes fixed to separate sites of a heart chamber, and the heart chamber is paced (or otherwise stimulated) by applying a pulse to one electrode and then the other after a specified time delay.

The present invention may be applied to distribute the pacing or non-excitatory stimulation of a heart chamber where the stimulated chamber may be either the atria or ventricles, or both. Furthermore, since the atria and ventricles both consist of paired chambers (i.e., right/left ventricle or atrium), the electrodes may be fixed to the stimulated chamber in a number of different ways. For example, in one embodiment, a ventricular pacemaker (or other electro-stimulatory device) has a set of pulse output configurations with each configuration comprising electrodes fixed to a single ventricle. In another embodiment, the available configurations may comprise electrodes fixed to both ventricles. In still another embodiment, each configuration is confined to one ventricle, but configurations are available for each ventricle so that stimulation pulses can be applied to either ventricle.

Pacing or non-excitatory stimulation may be distributed over the myocardium of a heart chamber by switching between pulse output configurations according to a switching algorithm. Switching between pulse output configurations can be made to occur on a beat-to-beat basis so that the stimulated site is alternated on every cardiac cycle or multiples of cycles. Alternatively, the configurations can be switched at periodic time intervals so that the pacing site is changed either rapidly (e.g., every minute) or over a much longer time period (e.g., weekly, monthly, etc.) depending upon the needs of the patient. The switching may also performed in accordance with a sensed physiological parameter so that the pulse output configuration is switched when the variable falls outside of a specified range. In one embodiment, cardiac output (as determined by, e.g., impedance measurement as described in U.S. Patent No. 4,674,518 issued to Salo et al., the disclosure of which is hereby incorporated by reference) is monitored, and the pulse output configuration is switched if it falls below a specified value. In another implementation, the depolarization following a pacing pulse is sensed at one or more sites at some distance from the pacing site or sites, and the time delay between the pacing pulse and the sensed depolarization is measured. The pulse output configuration is then switched if the time delay exceeds a specified value. In another embodiment, the mean or minimum heart rate is monitored (e.g., for a 24 hour period) and the pulse output configuration is switched if the rate exceeds a

threshold value. The specified parameter values used for switching the pulse output configuration is preferably programmable to suit the needs of individual patients. The change in the sensed physiological parameter that results when a particular pulse output configuration is switched on may also be used to select
5 the best pulse output configuration. The device may be programmed to go through a testing sequence in which pulse output configurations are alternately switched on and off, with the pulse output configuration then selected in accordance with which one produces the greatest improvement in the sensed parameter. For example, the pulse output configuration that produces the
10 highest cardiac output, the shortest measured time delay, or the lowest mean or minimum heart rate may be selected for pacing. Lastly, it may be desirable in some patients to simply configure the pacemaker to use only one pulse output configuration and switch to another configuration at a discretionary time using a telemetry interface.

15 A block diagram of a cardiac electro-stimulatory device having two ventricular stimulation channels is shown in Fig. 1. The control unit of the pacemaker is made up of a microprocessor 10 communicating with a memory 12 via a bidirectional data bus 13, where the memory 12 typically comprises a ROM (read-only memory) for program storage and a RAM (random-access
20 memory) for data storage. The control unit could also include dedicated circuitry either instead of, or in addition to, the programmed microprocessor for controlling the operation of the device. The control unit is capable of operating the device in a number of programmed modes where a programmed mode defines how pulses are output in response to sensed events and expiration of
25 time intervals. A telemetry interface 40 is also provided for communicating with an external programmer.

The pacemaker has atrial sensing/stimulation channels comprising electrode 34, lead 33, sensing amplifier 31, pulse generator 32, and an atrial channel interface 30 which communicates bidirectionally with a port of
30 microprocessor 10. The device also has two ventricular sensing/stimulation channels that include electrodes 24a-b, leads 23a-b, sensing amplifiers 21a-b, pulse generators 22a-b, and ventricular channel interfaces 20a-b where "a" designates one ventricular channel and "b" designates the other. For each

channel, the same lead and electrode are used for both sensing and stimulation. The channel interfaces 20a-b and 30 include analog-to-digital converters for digitizing sensing signal inputs from the sensing amplifiers and registers which can be written to by the microprocessor in order to output stimulation pulses, change the stimulation pulse amplitude, and adjust the gain and threshold values for the sensing amplifiers.

The device of Fig. 1 can be configured for practicing the present invention in one embodiment by programming its microprocessor to use only one ventricular stimulation channel during any one cardiac cycle, with the ventricular electrodes 24a and 24b fixed at either separate sites in one ventricle or fixed at sites in each ventricle. A selected stimulation channel thus constitutes a pulse output configuration that can be switched by the microprocessor according to a switching algorithm as described above. By switching between the stimulation channels, the stimulation is spatially and temporally distributed over the myocardium. The device as shown has two separate ventricular stimulation channels with separate pulse generators and electrodes for each channel. Thus, the selection of a stimulation channel is effected simply by the microprocessor commanding one or the other of the channels to deliver a pulse. In another embodiment, the two electrodes 24a-b could be connected to a common pulse generator through switching circuitry that switches from one electrode to another in accordance with an output from the microprocessor. Also, instead of separate ventricular stimulation electrodes 24a-b, a single bipolar electrode 50 as shown in Fig. 2 could be used, with the device having circuitry for switching the polarity of voltage pulses output to the electrodes so that either the tip 51 or ring 52 becomes the cathode. Thus if the electrode 50 is passed into the right ventricle with the tip 51 fixed at the apex and the ring 52 residing at the base, switching the polarity of the voltage pulses enables either the apex or base to be stimulated. Similarly, if the electrode 50 is passed into the left ventricle with the ring 52 residing in the coronary sinus and the tip 51 fixed in the myocardium through a cardiac vein, both basal and apical regions of the left ventricle can be stimulated.

Although the invention has been described in conjunction with the foregoing specific embodiments, many alternatives, variations, and

modifications will be apparent to those of ordinary skill in the art. Other such alternatives, variations, and modifications are intended to fall within the scope of the following appended claims.

WHAT IS CLAIMED IS:

1. A cardiac electro-stimulatory device for spatially and temporally distributing stimulation pulses to a heart chamber, comprising:
 - 5 a plurality of electrodes adapted for fixation to a heart chamber;
 - a plurality of defined pulse output configurations, wherein each pulse output configuration constitutes a subset of the plurality of the fixed electrodes;
 - and,
 - a control unit and pulse generating circuitry for outputting stimulation
 - 10 pulses to a selected one of the plurality of pulse output configurations in order to stimulate the heart chamber in response to sensed cardiac activity and lapsed time intervals in accordance with a programmed mode.
2. The device of claim 1 wherein the selected pulse output configuration is
- 15 switched to another configuration in accordance with a switching algorithm executed by the control unit.
3. The device of claim 1 wherein each pulse output configuration comprises one or more electrodes fixed to the heart chamber.
- 20 4. The device of claim 1 further comprising a telemetry interface and wherein the control unit is programmed to select one of the plurality of pulse output configurations in response to commands received from the telemetry interface.
- 25 5. The device of claim 1 wherein a pulse output configuration is further defined as a particular temporal sequence of pulses output to the electrodes making up the configuration.
- 30 6. The device of claim 2 wherein the control unit is programmed to switch the pulse output configuration on a beat-to-beat basis.

7. The device of claim 2 wherein the control unit is programmed to switch the pulse output configuration after a specified number of heartbeats.
8. The device of claim 2 wherein the control unit is programmed to switch
5 the pulse output configuration at a specified time interval.
9. The device of claim 2 wherein the control unit is programmed to switch the pulse output configuration in accordance with a sensed parameter.
- 10 10. The device of claim 9 wherein the sensed parameter is related to cardiac output.
11. The device of claim 9 wherein the device is a cardiac pacemaker and further wherein the sensed parameter is a sensed time delay of a depolarization
15 occurring in an area of the myocardium after delivery of a pacing pulse.
12. The device of claim 9 wherein the device is a cardiac pacemaker and further wherein the sensed parameter is the mean or minimum heart rate measured over a time interval.
- 20 13. The device of claim 1 wherein the plurality of electrodes comprises a bipolar electrode and further comprising circuitry for switching the polarity of pulses output to the electrode, each selected polarity thus constituting a pulse output configuration.
- 25 14. The device of claim 1 further comprising a separate pulse generators for each electrode.
15. A method for electrically stimulating a heart chamber, comprising:
30 outputting stimulation pulses to a subset of a plurality of electrodes fixed to the heart chamber in response to sensed cardiac activity and lapsed time intervals in accordance with a programmed mode, wherein the subset of

electrodes to which pulses are output is defined by a pulse output configuration;
and,

switching the pulse output configuration in accordance with a switching
algorithm so that stimulation pulses are output to a different subset of the fixed
5 electrodes.

16. The method of claim 15 wherein the heart chamber is either the atria or
the ventricles, and the plurality of electrodes fixed to the heart chamber are fixed
to one of the paired atria or ventricles.

10

17. The method of claim 15 wherein the stimulated heart chamber is either
the atria or the ventricles, the plurality of electrodes fixed to the heart chamber
are fixed to both of the paired atria or ventricles, and a pulse output
configuration may comprise electrodes fixed to either of the paired atria or
15 ventricles.

18. The method of claim 15 wherein the switching algorithm comprises
switching the pulse output configuration on a beat-to-beat basis.

20 19. The method of claim 15 wherein the switching algorithm comprises
switching the pulse output configuration at a specified time interval.

20. The method of claim 15 wherein the switching algorithm comprises
switching the pulse output configuration in response to a command received by
25 the device through a telemetry interface.

21. The method of claim 15 wherein the switching algorithm comprises
switching the pulse output configuration in accordance with a parameter sensed
by the device.

30

22. The method of claim 15 wherein the switching algorithm comprises
switching the pulse output configuration after a specified number of heart beats.

23. The method of claim 15 wherein a pulse output configuration is further defined as a temporal sequence of pulses output to the fixed electrodes during a cardiac cycle.
- 5 24. The method of claim 15 wherein the stimulation pulses are output to a bipolar electrode having tip and ring electrodes fixed to a heart chamber, and further comprising switching the pulse output configuration by alternating the polarity of the delivered pulses.
- 10 25. The method of claim 24 wherein the bipolar electrode is passed through the coronary sinus of a patient such that the tip of the electrode is fixed to the apical region of the left ventricle while the ring is in electrical contact with a more superior region of the left ventricle.
- 15 26. The method of claim 24 wherein the bipolar electrode is passed into the right ventricle of a patient such that the tip of the electrode is fixed to the apical region of the left ventricle while the ring is in electrical contact with a more superior region of the ventricle.

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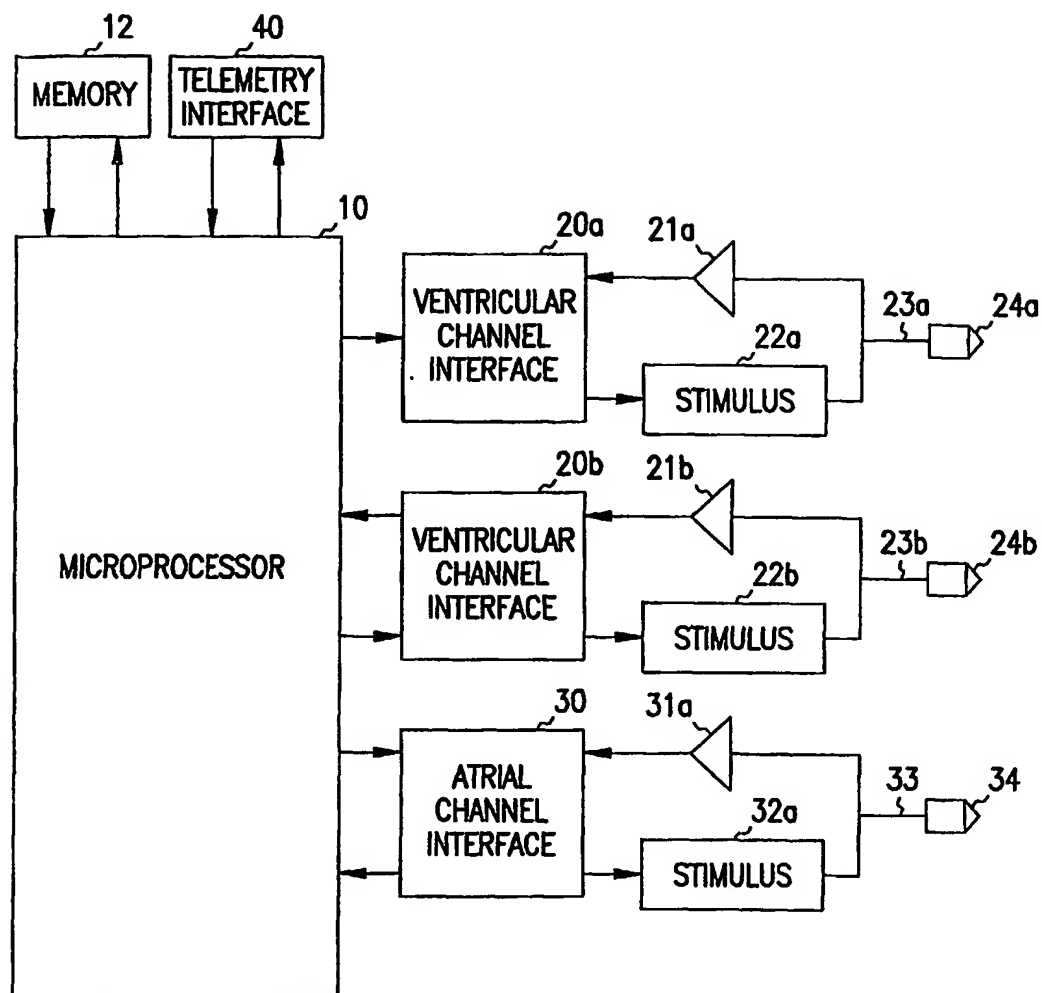


FIG. 1

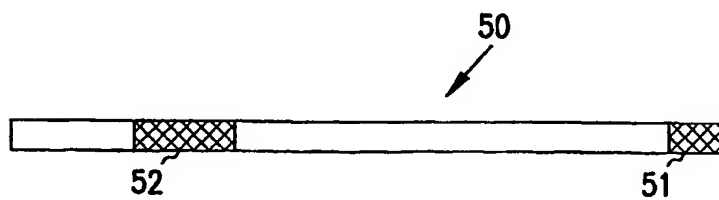


FIG. 2

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